

Respiratory Mechanics

Critical Care Medicine Specialty Board Tutorial

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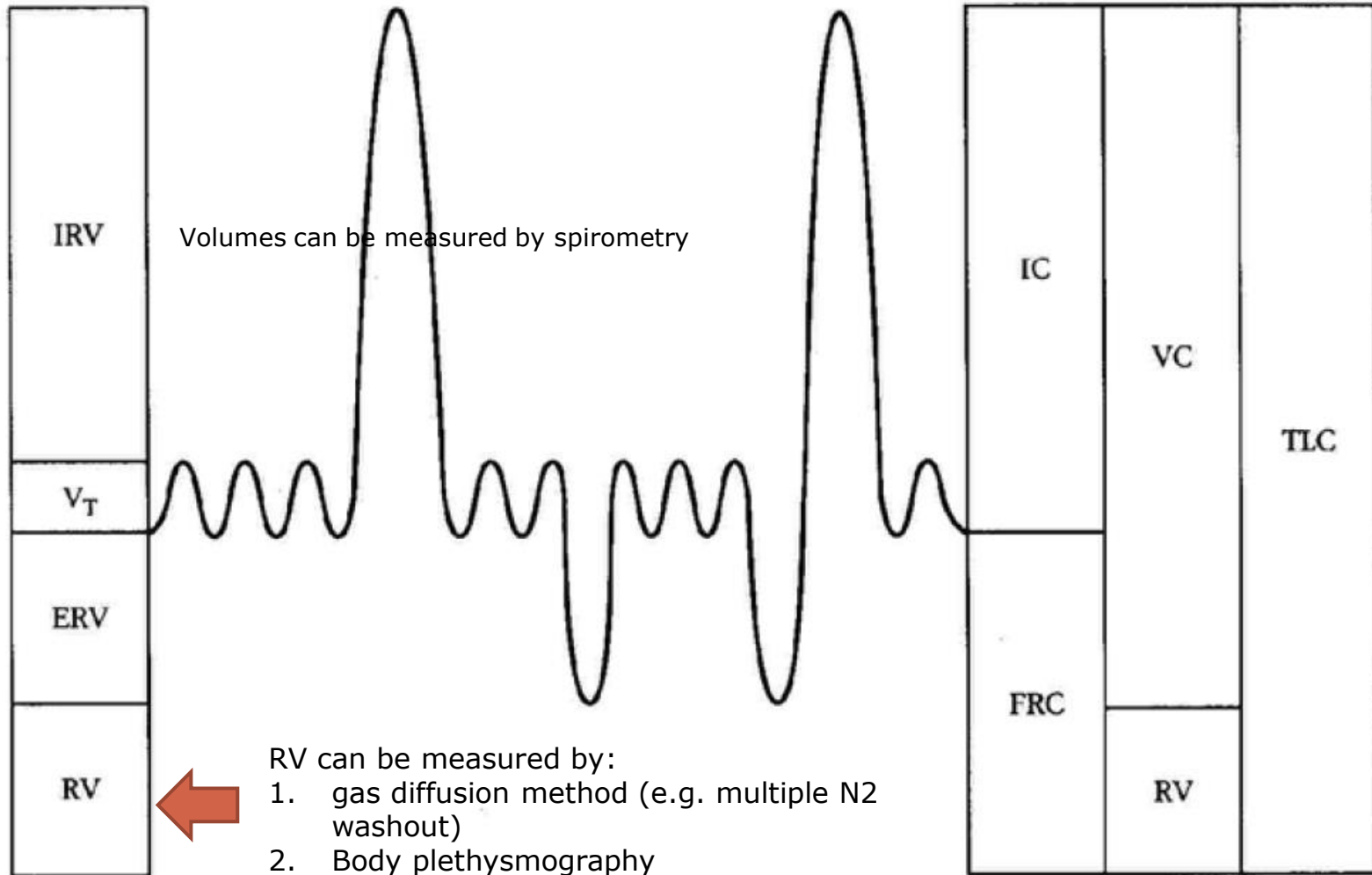
This lecture covers:

1. Basic knowledge: volume, flow, pressure
2. Lung parenchymal condition: compliance
3. Airway condition: FEV1/FVC, Resistance, Flow pattern
4. Chest wall condition: Chest wall compliance
5. Interaction of all factors: PV curve of whole system, Time constant, Flow-time curve, Flow-volume curve, Static and Dynamic hyperinflation, intrinsic PEEP, EELV
6. Work of breathing: Campbell diagram, Pressure-Time Product (PTP)
7. The force of breathing: SVC, FVC, MIP, MEP, Trans-diaphragmatic pressure, P0.1
8. Other application: Transpulmonary pressure

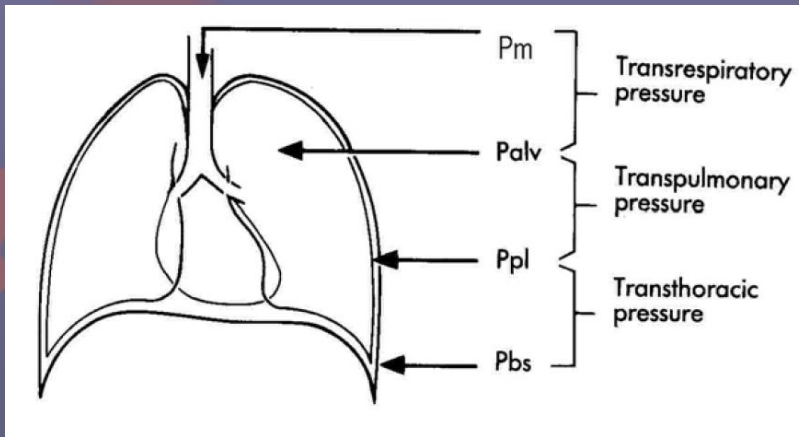
The background of the slide is a solid dark blue-grey color. It is decorated with several stylized autumn leaves in shades of brown and orange, scattered primarily along the left and right edges.

Basic knowledge: Volume, flow,
pressure

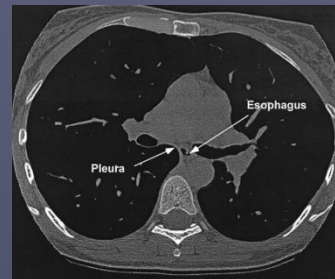
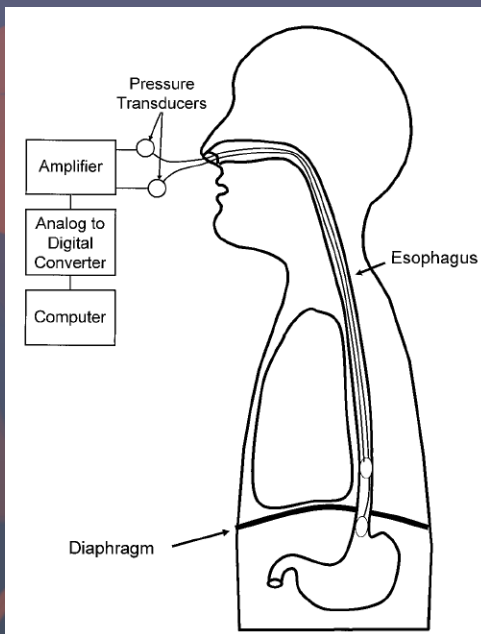
Lung volumes



Basic primary and derived pressures



Others: P_{es} and $P_{gastric}$

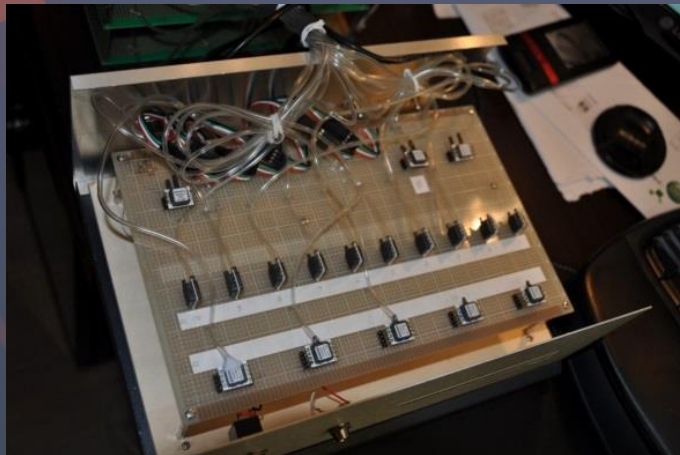


Airflow and Pressures

- Airflow is measured at the airway opening
 - With a pneumotach
 - Integration of flow with time is volume
- Primary pressures
 - P_{bs} (body surface) = $P_{atm} = 0$
 - $P_{pl} = P_{es}$
 - P_m (mouth) = P_{aw} at Y-end (during MV)
 - $P_{gastric}$
- Derived pressures
 - Trans-resp system $P = P_{aw} - P_{atm}$
 - $P_{alv} = P_{aw}$ during no flow
 - Transpulmonary $P = P_{alv}$ (or P_{aw} during no flow) - P_{es}
 - Transthoracic $P = P_{es} - P_{atm}$

Actual measurement

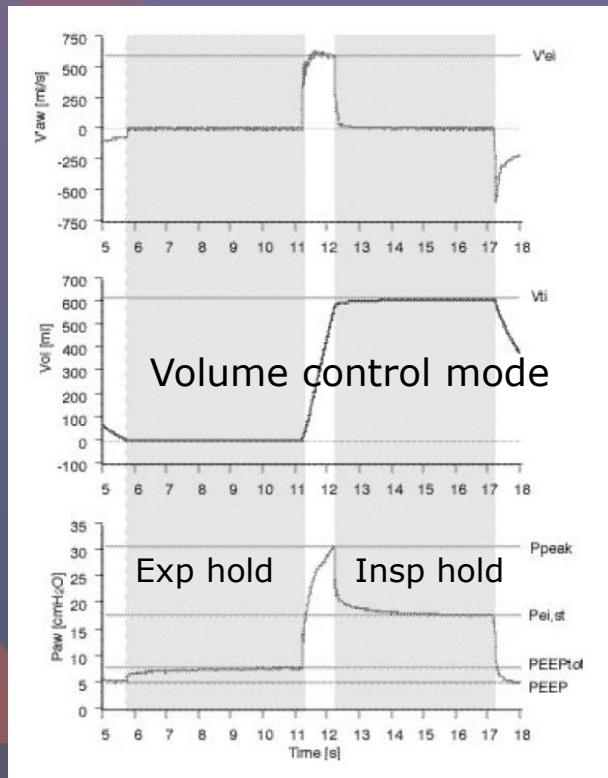
- Flow & pressures
 - Pneumotach & airway pressure transducer placed distal to Y-connector
 - Esophageal balloon catheter
 - Signals transformed by an analogue-to-digital converter, recorded by LabVIEW software
- Edi signal
 - Acquired from ventilator at 100 Hz via a RS232 interface to the ServoTracker software
- Time-aligned and analyzed off-line



Lung and chest wall conditions: Compliance

- Two situations:
 - Dynamic compliance (actively breathing, e.g. at peak flow)
 - Static situation (during no flow condition, e.g. at plateau pressure obtained by inspiratory pause; or in a totally relaxed patient, P and V obtained point-by-point)
- Formulae
 - Compliance = $\Delta \text{volume} / \Delta P$ (*P is across unit to be measured, unit of compliance is ml/cmH₂O*)
 - $C_{rs} = V_t / (\text{Trans-resp system } P \text{ at end-insp} - \text{Trans-resp system } P \text{ at end-exp})$
 - $C_{lung} = V_t / (\text{Trans-pulmonary } P \text{ at end-insp} - \text{Trans-pulmonary } P \text{ at end-exp})$
 - $C_{cw} = V_t / (\text{Trans-thoracic } P \text{ at end-insp} - \text{Trans-thoracic } P \text{ at end-exp})$
 - Elastance = $1/\text{Compliance}$

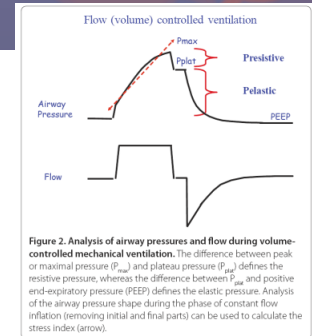
Compliance and Resistance measurement of the respiratory system (Double Occlusion Method, paralyzed patient)



$$\text{Static compliance} = \text{TV} / (\text{Pplat} - \text{PEEP})$$

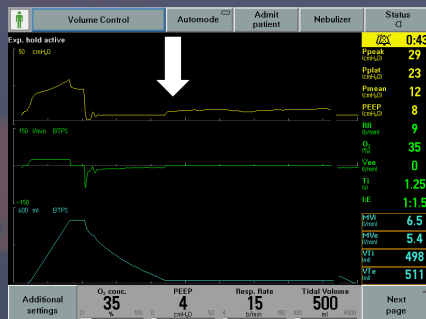
The respective data are:

V'e _i	0.6	l/s
V _{ti}	610	ml
P _{peak}	31	cmH ₂ O
P _{ei,st}	17.5	cmH ₂ O
PEEP _{tot}	7.5	cmH ₂ O
PEEP _e	5	cmH ₂ O



Based on these data, we can calculate R_{max}, C_{stat}, and PEEPi according to the formulas of § 4.2., as follows :

C _{stat}	610 / (17.5 - 7.5)	=	61	ml/cmH ₂ O
R _{max}	(31 - 17.5) / 0.6	=	22.5	cmH ₂ O/l/s
PEEP _i	7.5 - 5	=	2.5	cmH ₂ O



Exp hold

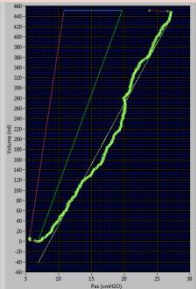
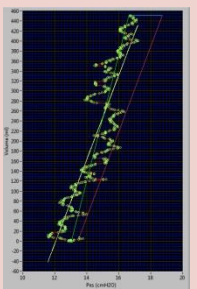
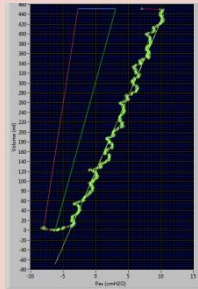


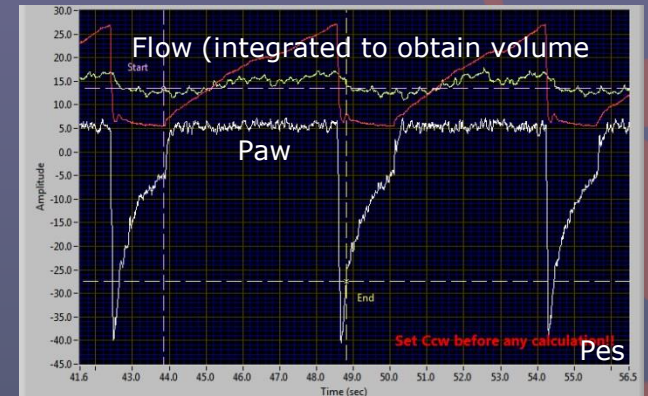
Insp hold

- Compliance if of:
 - The whole respiratory system (tubings, ETT, patient) if pressure port is in ventilator
 - The patient and ETT, if pressure port is at Y-end
 - The patient only, if pressure port is at carina (beyond ETT tip)

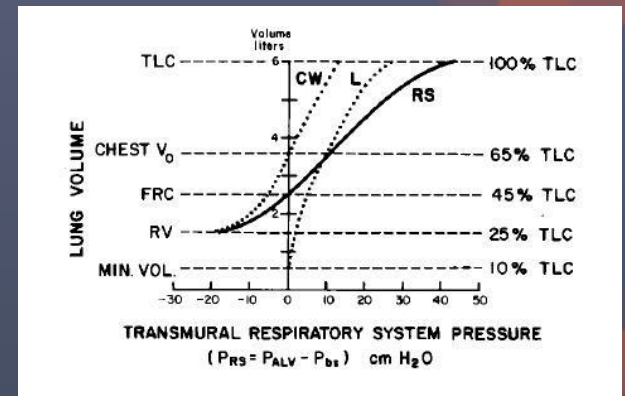
Full compliance study of respiratory system, lungs and chest wall in research setting (paralyzed patient)

$$\text{Formula: } 1/C_{\text{lung}} = 1/C_{\text{total}} - 1/C_{\text{cw}}$$

Patient	Total compliance (ml/cmH2)	Chest wall compliance	Lung compliance	Lung (calculated as $C_{\text{total}} - C_{\text{cw}}$)
CHF	23.6  Paw $C_{\text{total}} = \Delta(P_{\text{aw}} - P_{\text{atm}}) / \Delta V$	84  Pes $C_{\text{cw}} = \Delta(P_{\text{es}} - P_{\text{atm}}) / \Delta V$	30.5  Transpul P = $P_{\text{aw}} - P_{\text{es}}$ $C_{\text{lung}} = \Delta(P_{\text{aw}} - P_{\text{es}}) / \Delta V$	32.8 $1/C_{\text{lung}} = 1/C_{\text{total}} - 1/C_{\text{cw}}$
COPD	84.5	195	142	149

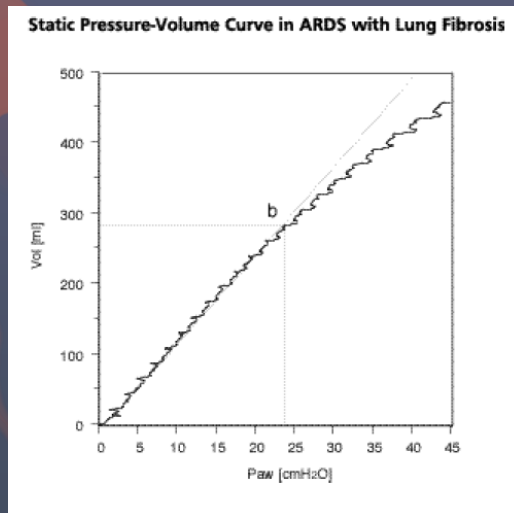
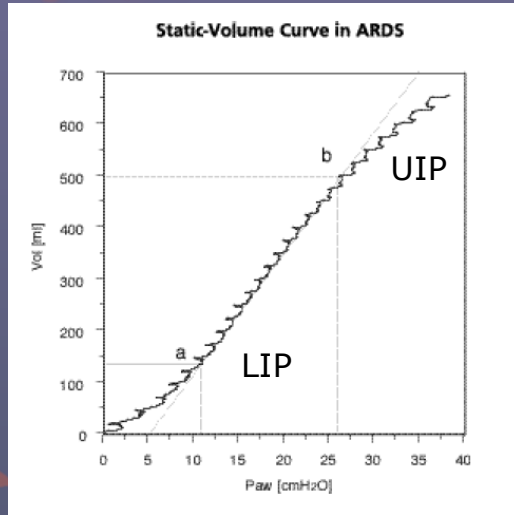


Time tracings of the paralyzed CHF patient



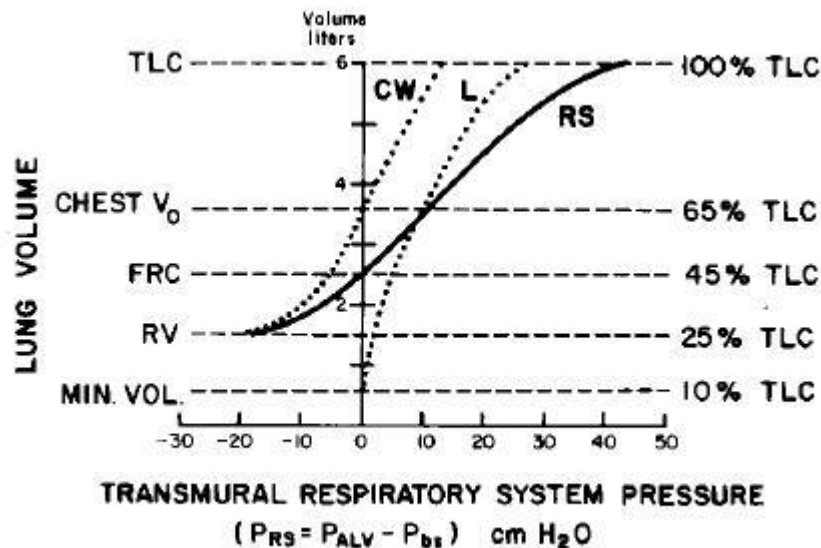
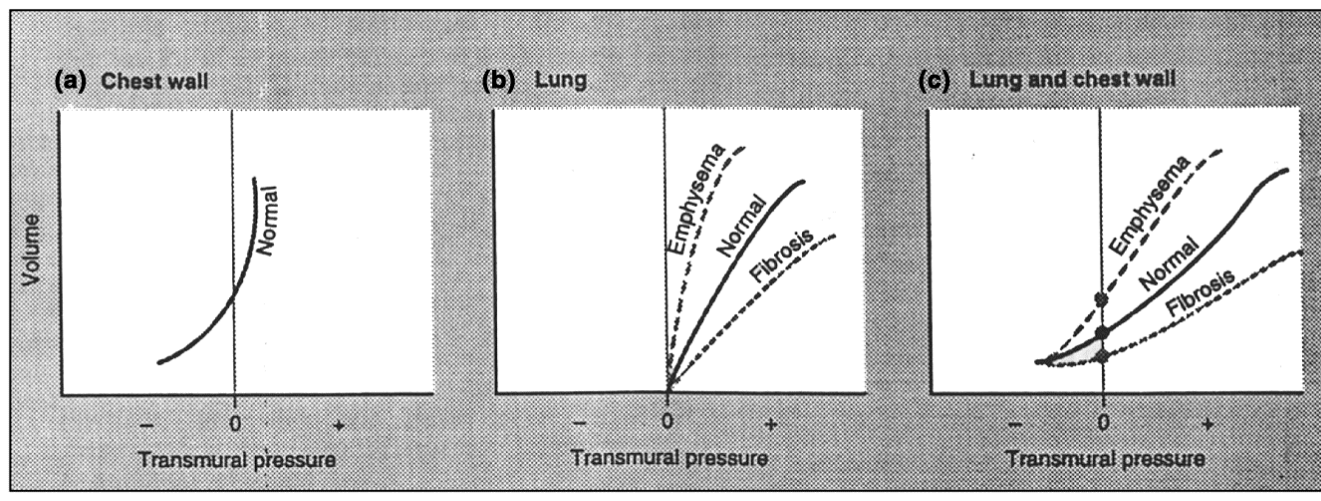
Static relaxation pressure-volume curve

Compliance measurement of the respiratory system in research situation: Static PV curve by the Low Constant Flow method



- Compliance is of the whole respiratory system if Paw is used
- Tiny irregularities correspond to cardiac oscillations
- Slope of straight portion = best compliance of the resp system
- ARDS: Lower (LIP) and upper inflection points (UIP) in ARDS
- Lung fibrosis: No lower inflection point implies no recruitable alveoli, B represents start of upper inflection zone and implies overdistension

Static Relaxation Pressure-Volume Curves



Grinnan and Truwit Critical Care 2005 9:472-484
doi:10.1186/cc3516

- At lung volumes above ~70% of the vital capacity, the chest wall no longer tends to spring out but instead to spring in.
- relaxation pressure of the lung plus chest wall is simply the sum of the relaxation pressures of the two components.

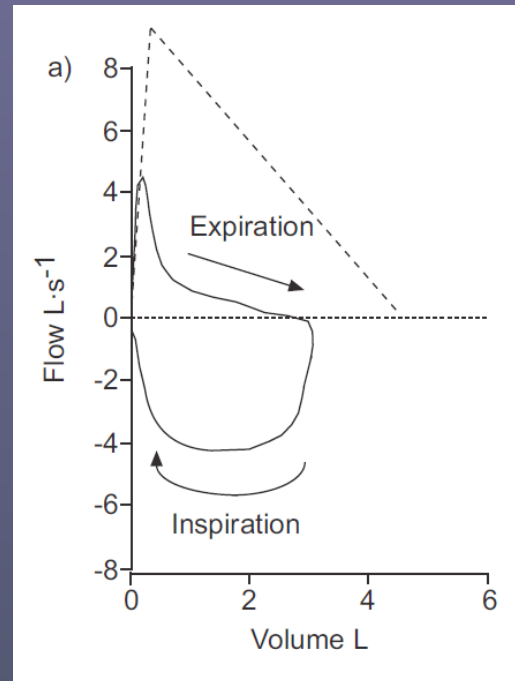
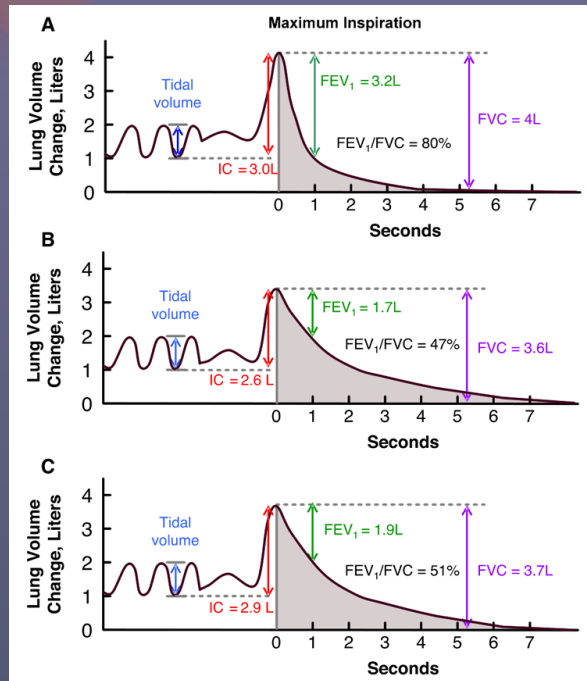
Application: Open lung tool to look for the best dynamic compliance for PEEP setting



Airway condition

- Awake patient: FEV₁/FVC by forced spirometry
- Intubated patient: Resistance by inspiratory hold

Forced spirometry: in non-intubated patients



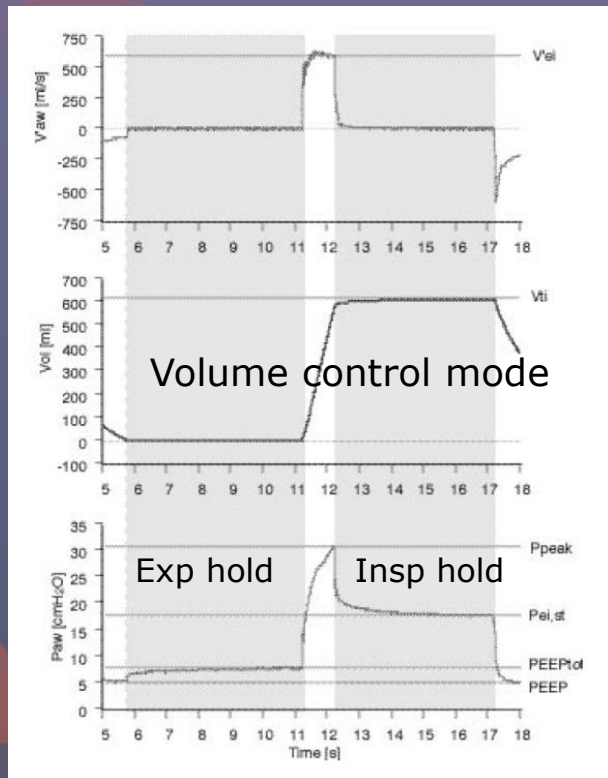
1. FEV1/FVC ratio

- If <70%, means there is airflow obstruction (GOLD Guideline criteria)
- If <lower 5th percentile, means there is airflow obstruction (more stringent statistical criteria, HK local reference equation: Ip MS et al. Updated spirometric reference values for adult Chinese in Hong Kong and implications on clinical utilization. Chest. 2006 Feb;129(2):384-92.)

2. FEV1

- The predicted percentage reflects the severity of the airflow obstruction, if present
- Severity of obstruction is based on FEV1
 - < 35% predicted: severe
 - 35 – 50% predicted: moderate
 - 50 – 80% predicted: mild

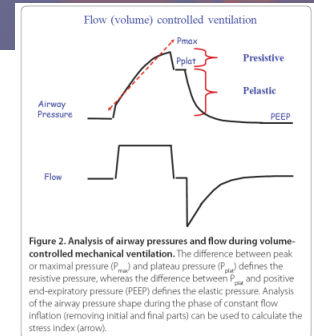
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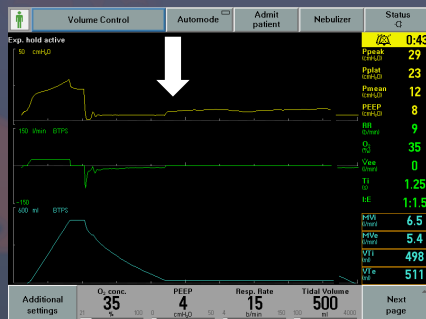
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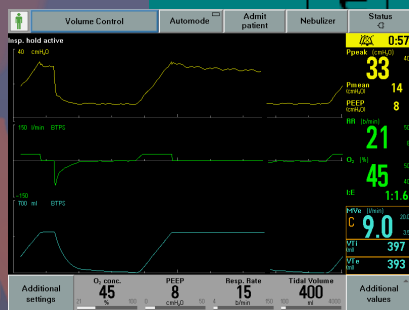
Exp hold



Insp hold

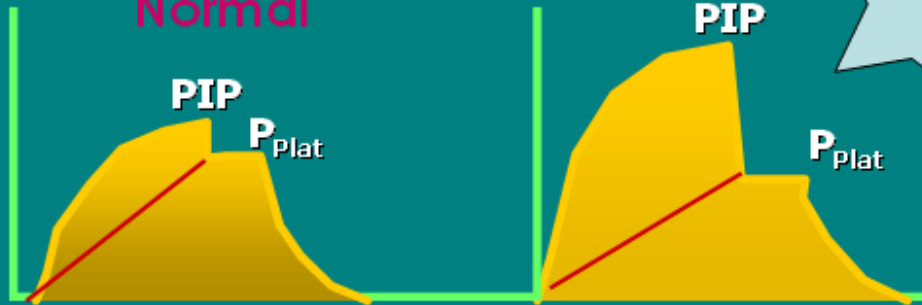
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Inspiratory hold, volume control mode: Distinguish among resistance, compliance and flow problem



PIP vs P_{plat}

Normal



High R_{aw}

PIP

P_{Plat}

PIP增加
P_{pla}不變
PIP-P_{pla}增加
氣道阻力增加
Ex: Asthma,
COPD

High Flow

PIP

P_{Plat}

PIP增加
P_{pla}沒變
阻力也增加。
但是因吸氣
時間縮短，
表流速太高

Low Compliance

PIP

P_{Plat}

PIP增加
P_{pla}增加
但PIP-P_{pla}
沒變表阻力
沒增加，是
順應性減低
Ex: ARDS,
PN

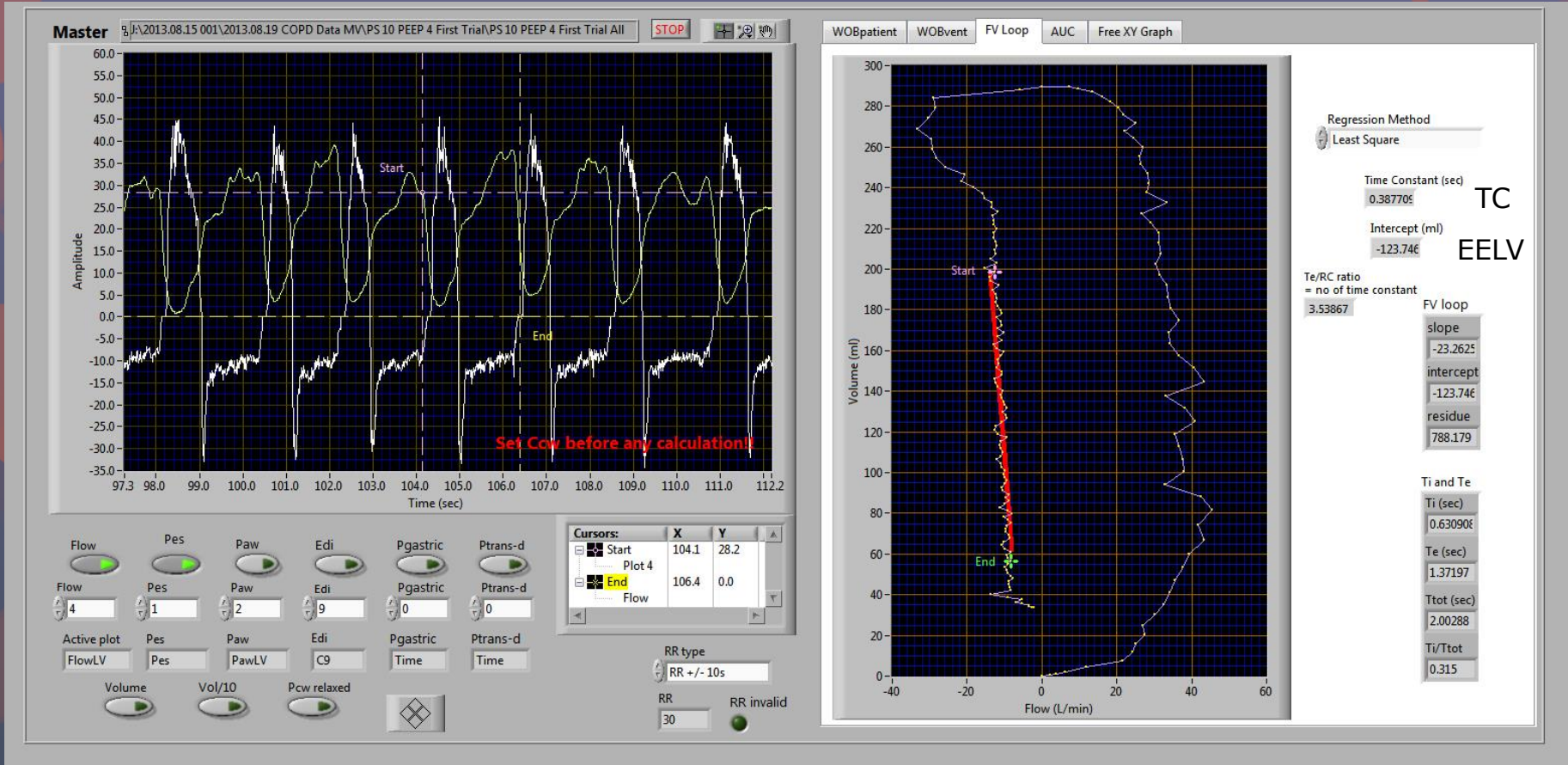
Time (sec)

Interaction of all factors

Interaction of of lung, airway and chest wall: PV curve of whole system, Time constant, Flow-time curve, Flow-volume curve, Static and Dynamic hyperinflation, intrinsic PEEP, EELV

Time Constant

- = Resistance x Compliance = (delta P/Flow) x (delta vol / delta P)
- = delta Volume/Flow (can be read at expiration of passive flow-volume loop)



Flow-Volume Loop in an actively breathing COPD Patient: Shows Time Constant and End-Exp Lung Volume (EELV)

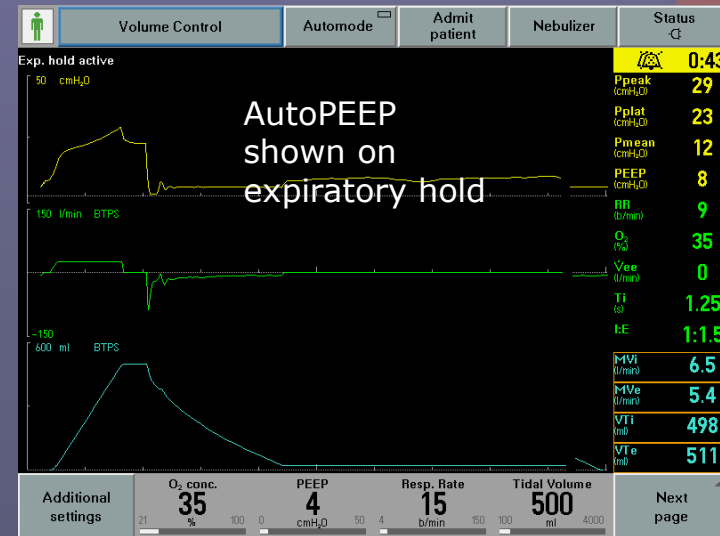
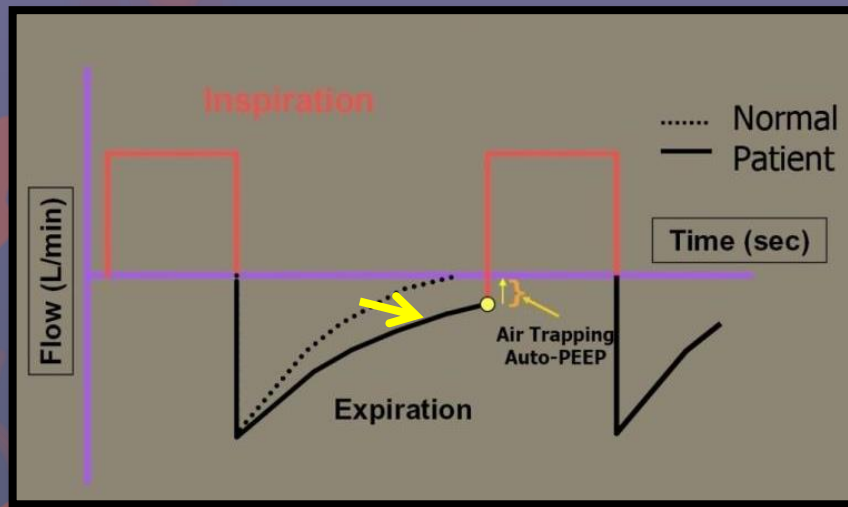
Clinical implications

Duration of step change in pressure (s)	Resulting change in volume (% of $\Delta\text{Vol}_{\text{max}}$)
1 x Time Constant	63
2 x Time Constant	86.5
3 x Time Constant	95
4 x Time Constant	98
5 x Time Constant	99
Infinite x Time Constant	100

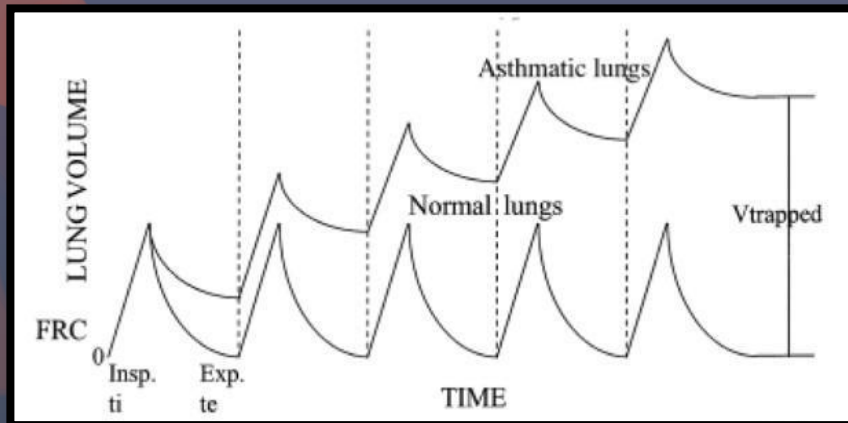
- To avoid hyperinflation, we must allow an expiratory time of 4, or at least 3, time constants.

	Resistance	Compliance	RC	Te required
ARDS	Low	Low	Low	Low
Acute Asthma	High	Normal	High	High
Emphysema	High (exp)	High	High	High

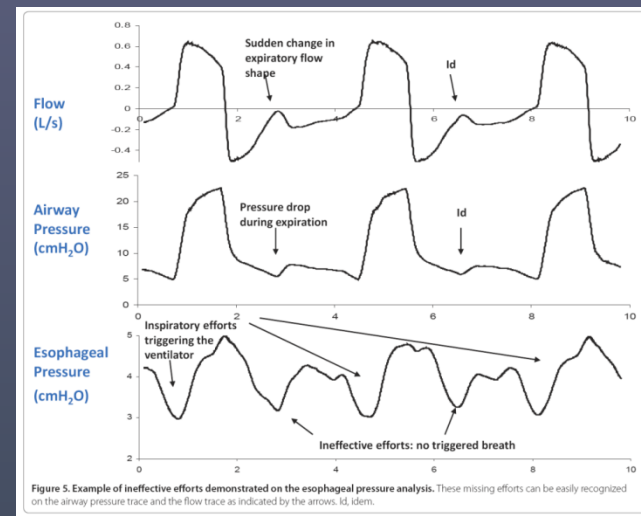
Ventilator tracing of incomplete emptying due to AFO



Flow vs time curve

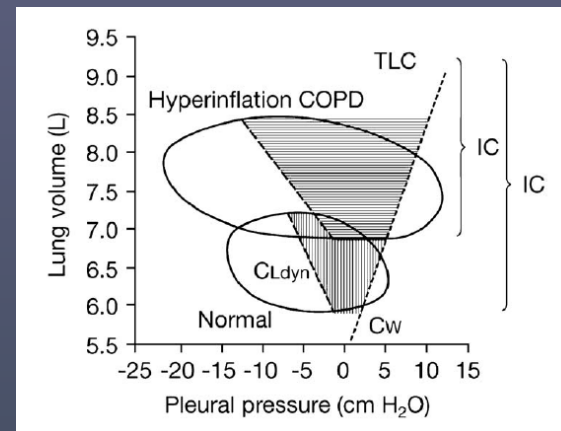
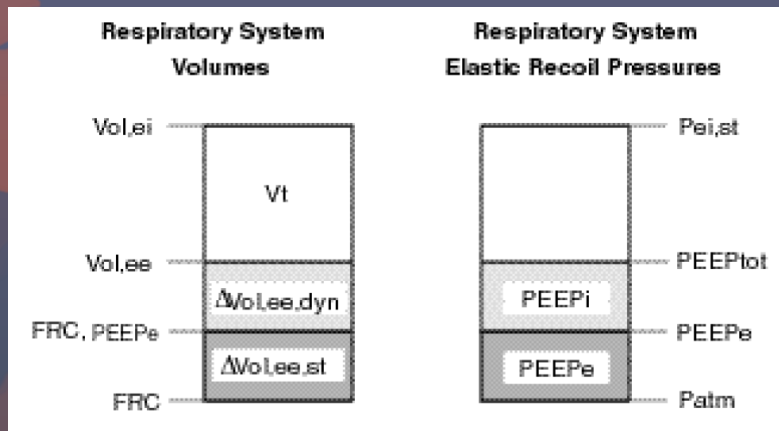
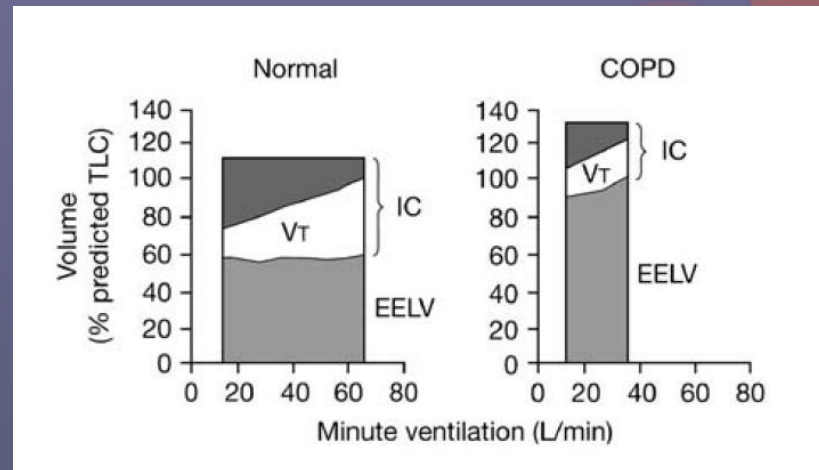
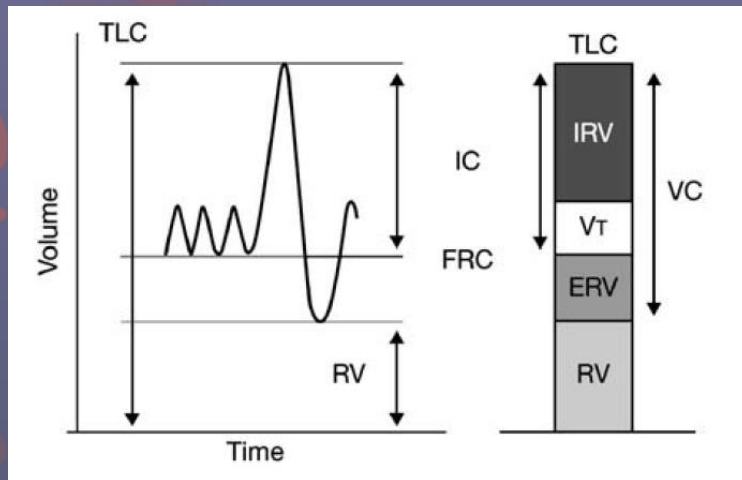


Actually what happens is: Volume vs time curve (without zero resetting before each breath)



O'Donnell DE, et al. Eur Res Rev 2006

Terminology

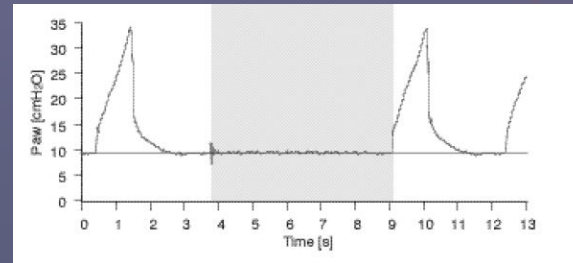
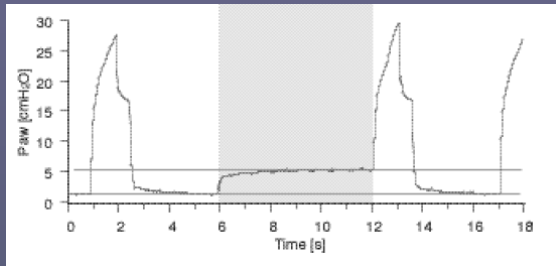


$PEEP_{tot} = PEEPe + PEEPi$; i.e. $PEEPi = PEEP_{tot} - PEEPe$

Static and dynamic intrinsic PEEP: Static and dynamic refers to the method of measurement, not whether the patient is actively breathing or paralyzed

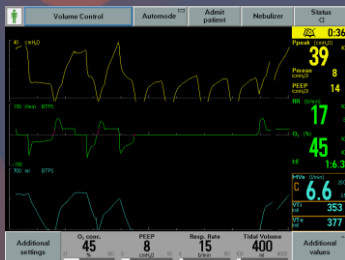
Static intrinsic PEEP

- In a paralyzed patient
 - End-exp occlusion manoeuvre (i.e. Based on $PEEP_i$, $st = PEEP_{tot} - PEEP_e$)

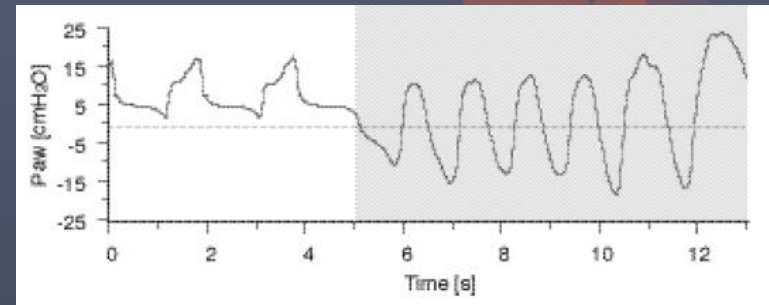
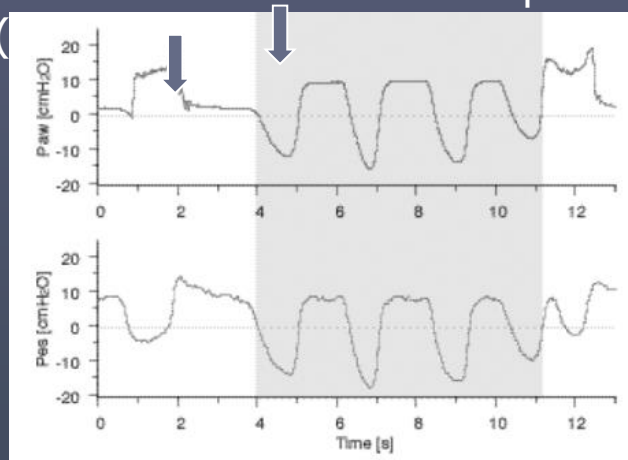


Zero $PEEP_i$

- In actively breathing patient
 - 7-sec end exp occlusion manoeuvre, $PEEP_{tot}$ is the Paw between two successive periods of muscular activation



Real-life tracing



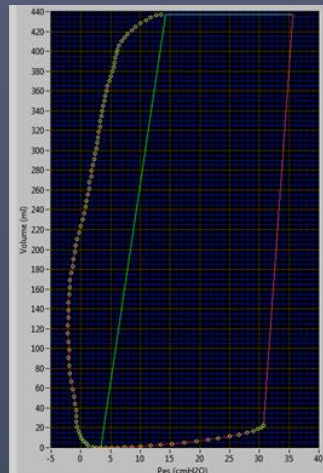
Pseudo-relaxation period too short and not flat:
Not fit for analysis

Dynamic PEEPi

- Based on Pes drop to initiate flow, therefore refers to actively breathing patients only
- = Negative deflection of Pes from the onset of inspiratory effort to onset of flow from zero

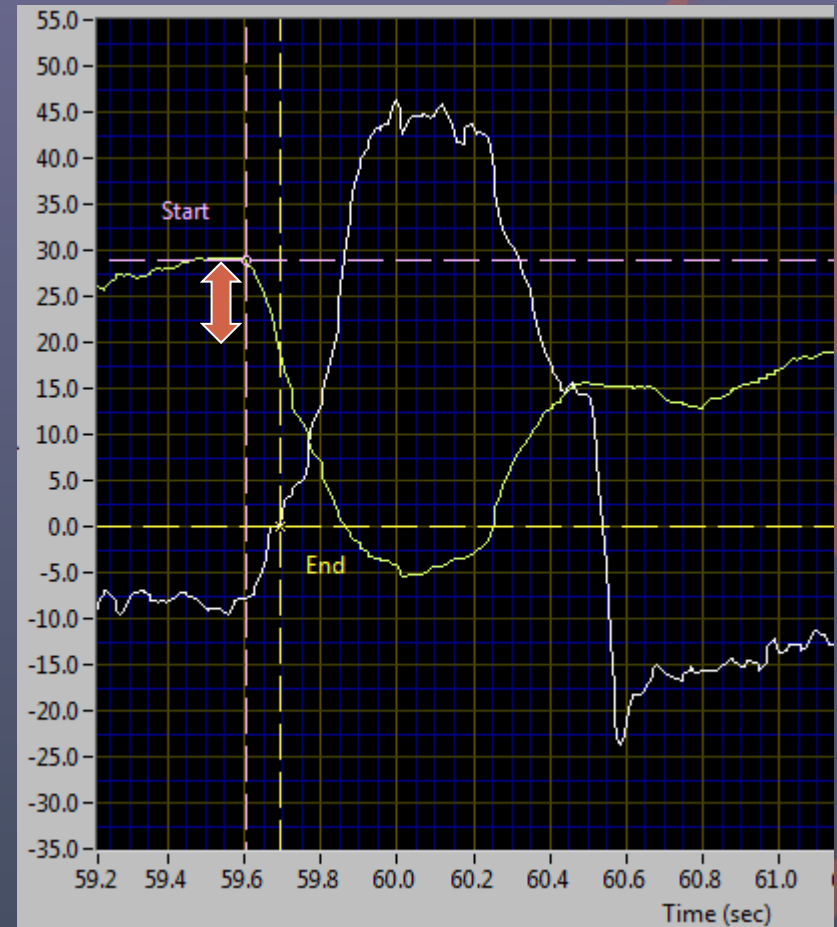
TV

When displayed in a Pes-Vol loop:



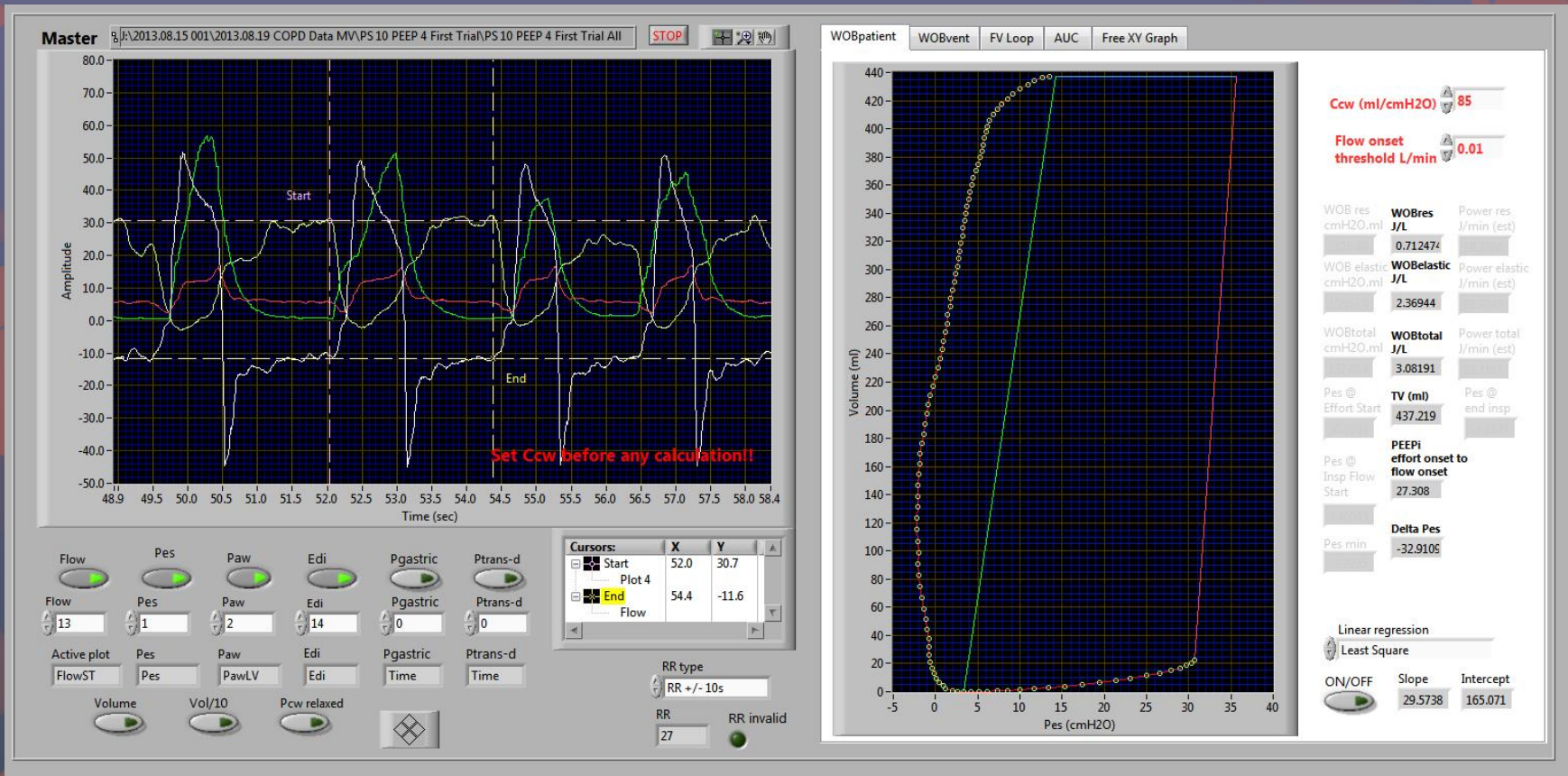
←→
Pes generated to initiate flow

Pressure (cmH2O) or Flow (L/min)



Dynamic PEEPi

Based on the Pes drop to initiate flow, in a spontaneously breathing patient



Work of breathing

Campbell's Diagram, Pressure-Time Product

Campbell's Diagram

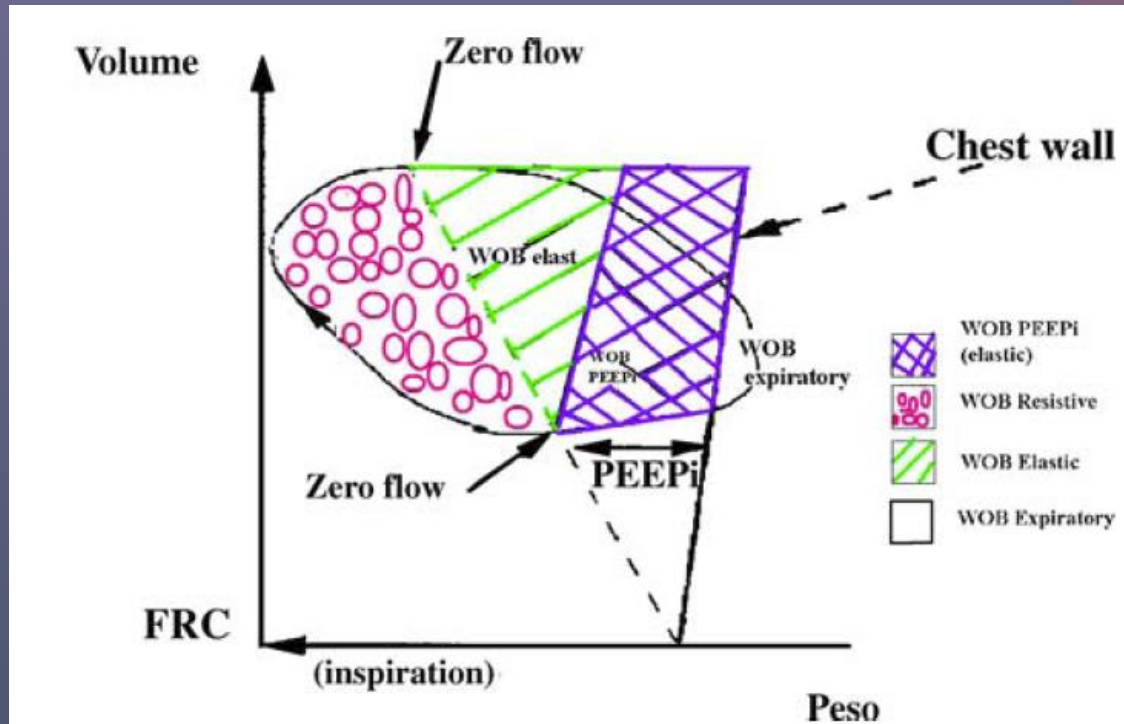


Fig.1 Campbell's diagram. Work of breathing measured by the esophageal pressure: resistive WOB (W_{resist}), elastic WOB (W_{elast}), WOB related to active expiration ($WOB_{expiratory}$) and WOB related to intrinsic PEEP (W_{PEEP_i}). *Chest wall*: this thick line (the chest wall compliance) represents the pleural (esophageal) pressure obtained when muscles are totally relaxed and lung volume increases above functional residual capacity, measured in static conditions

Campbell's Diagram in practice

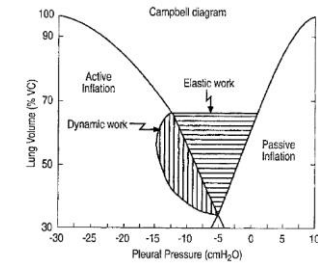
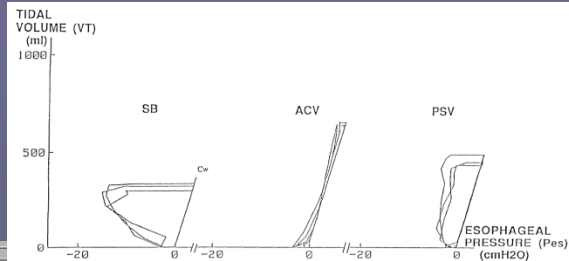
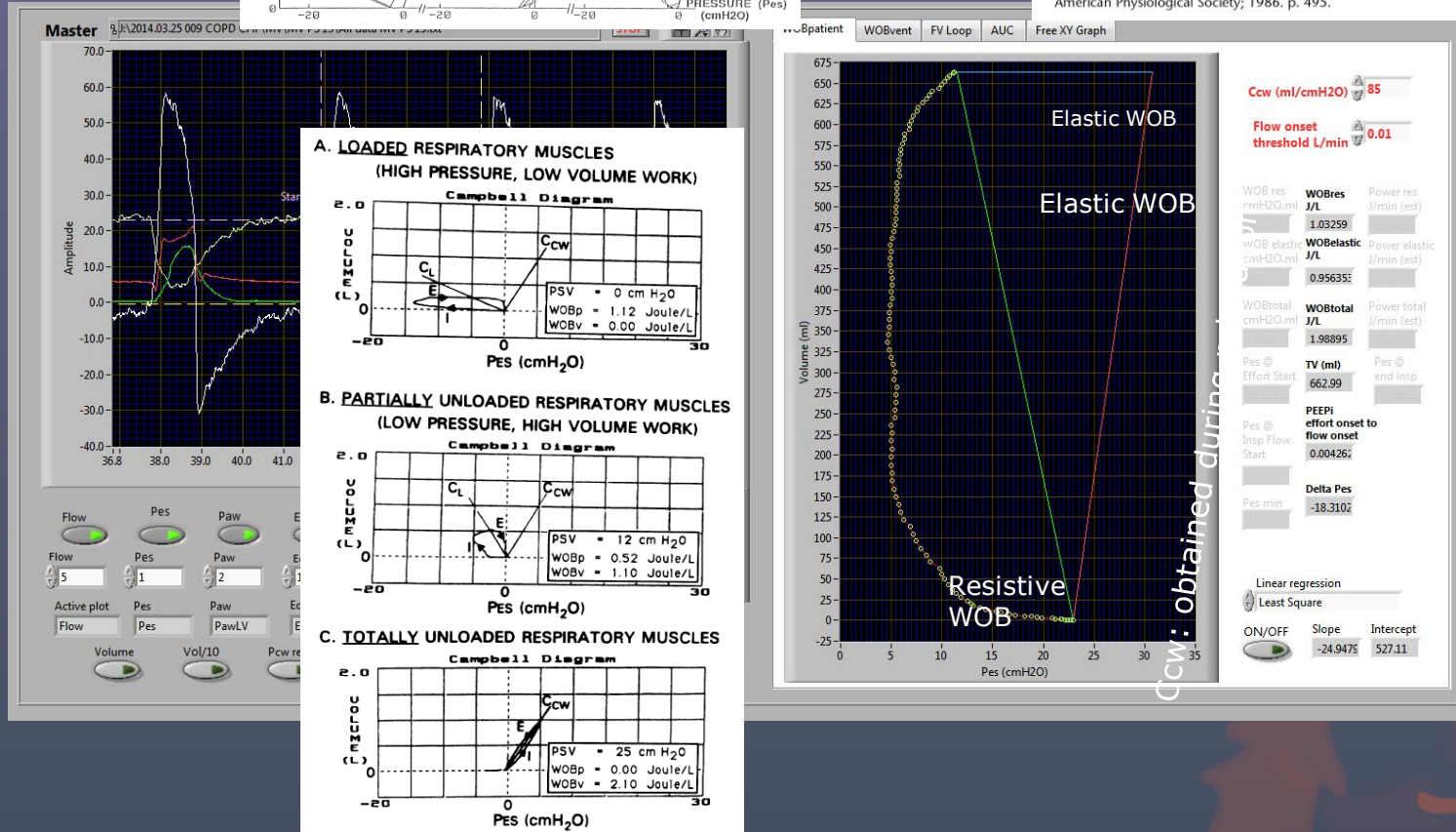
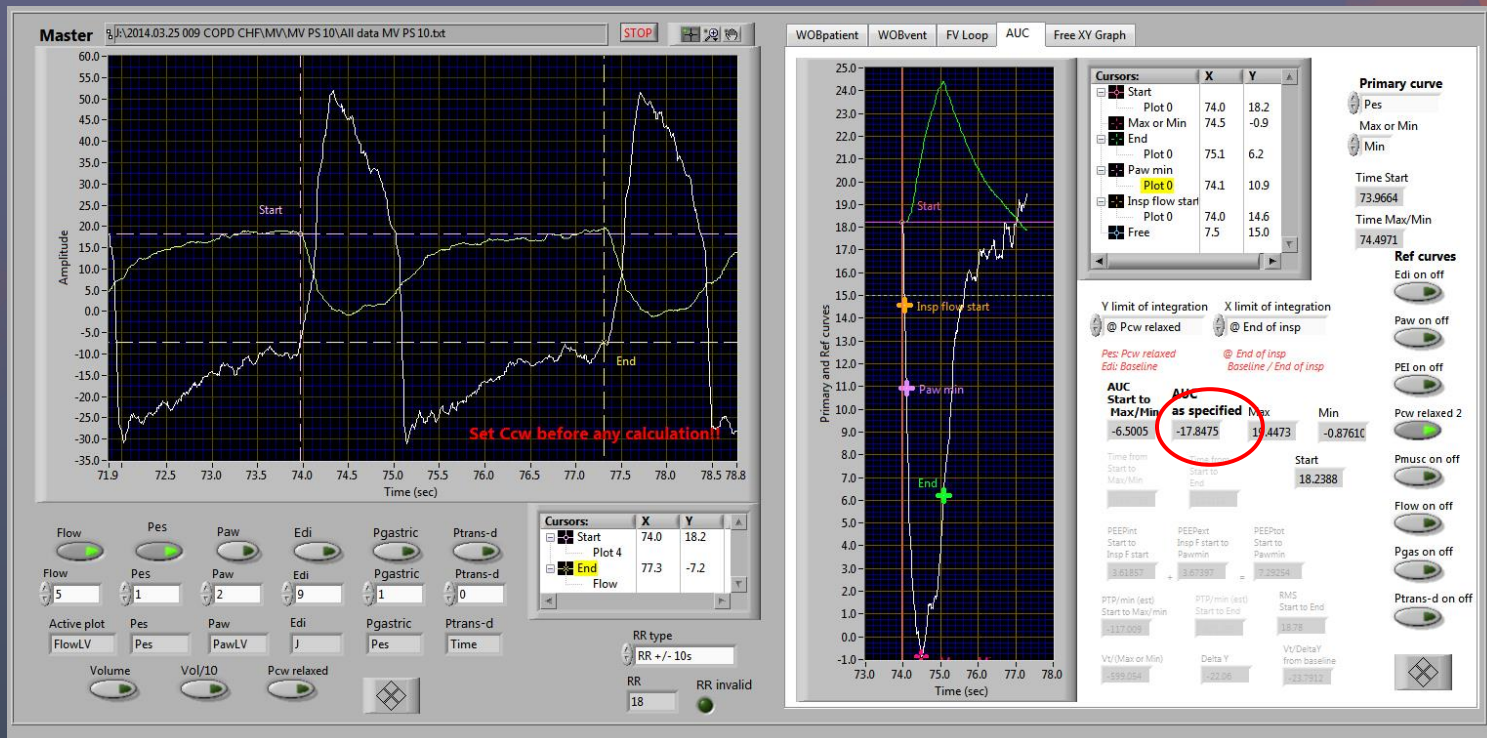


Figure 2. Campbell diagram. Graphical analysis of the work done during a breathing cycle by the inspiratory muscles. Vertical hatching: Work done to overcome flow resistance of the lungs. Horizontal hatching: Work done to overcome elastance of the lungs and chest wall. Modified by permission from Macklem PT, Mead J, editors. Handbook of physiology. Vol. 3: The respiratory system, Part 3. Bethesda, MD: American Physiological society; 1986. p. 495.



Pressure-time product

- PTP that reflects the exertion of the respiratory muscles for inspiration (PTP_{insp,pat}) = time interval between the inspiratory effort start and the end of the inspiratory phase of a cycle
 - $PTP/breath \times RR = PTP \text{ per minute (cmH}_2\text{O.s/min)}$



The Force of Breathing

SVC, FVC, MIP, MEP, Trans-diaphragmatic pressure, P0.1

Monitoring



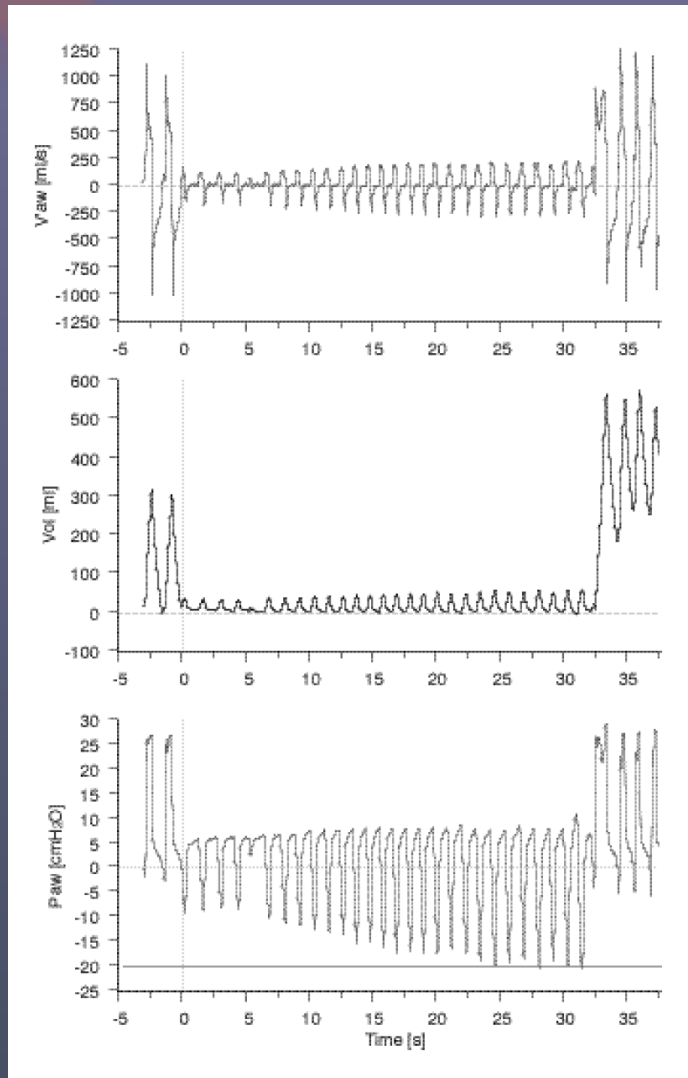
SVC, MIP, MEP in spontaneously breathing patient

	Normal	Predictive of respiratory failure
Slow Vital Capacity (SVC)	50 ml/kg	< 20 ml/kg
Maximal Inspiratory Pressure (MIP) – from RV	- 70 cm H ₂ O	Less neg than – 30 H ₂ O
Maximal Expiratory Pressure (MEP) -from TLC	150 cm H ₂ O	< 40 cm H ₂ O

MIP in intubated patient

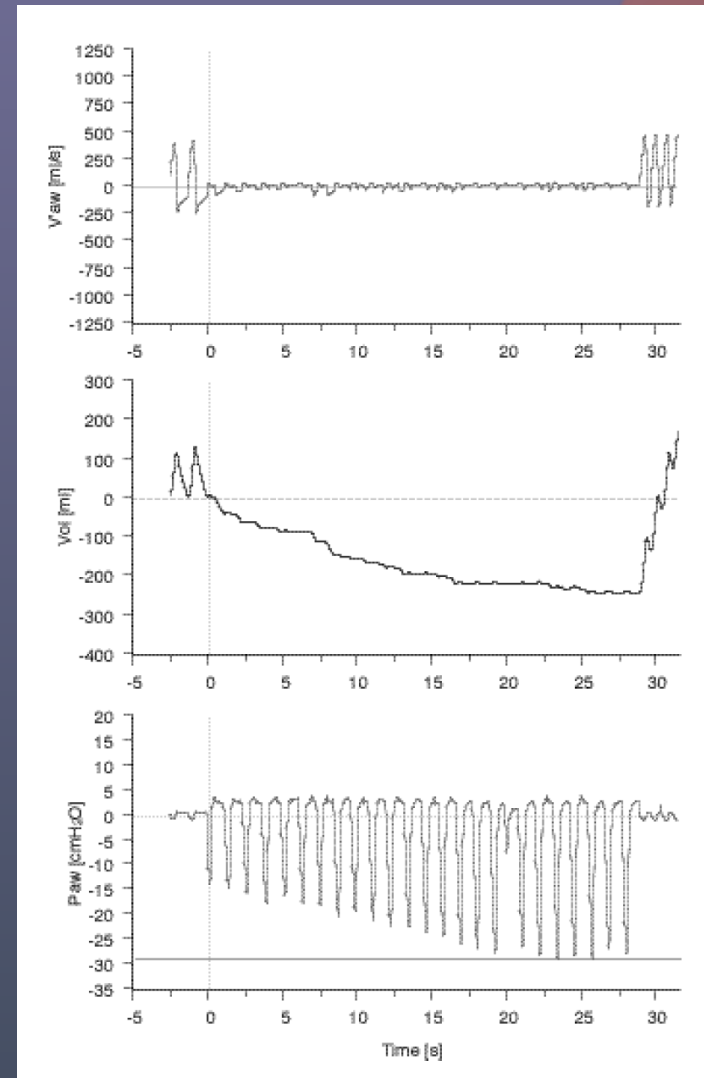
- Negative pressure generated by the inspiratory muscles during a maximal inspiratory effort, performed during temporary occlusion of the airway opening
- = PIMax, = NIP, expressed as a positive number
- Unit is cmH₂O
- Two methods (after removal of any PEEPe applied by the ventilator):
 1. at the end-expiratory volume
 2. below the end-expiratory volume

Method 1



End-expiratory occlusion

Method 2



Requires a one-way valve that limit occlusion to inspiration only, but free to exhale

Transdiaphragmatic pressure

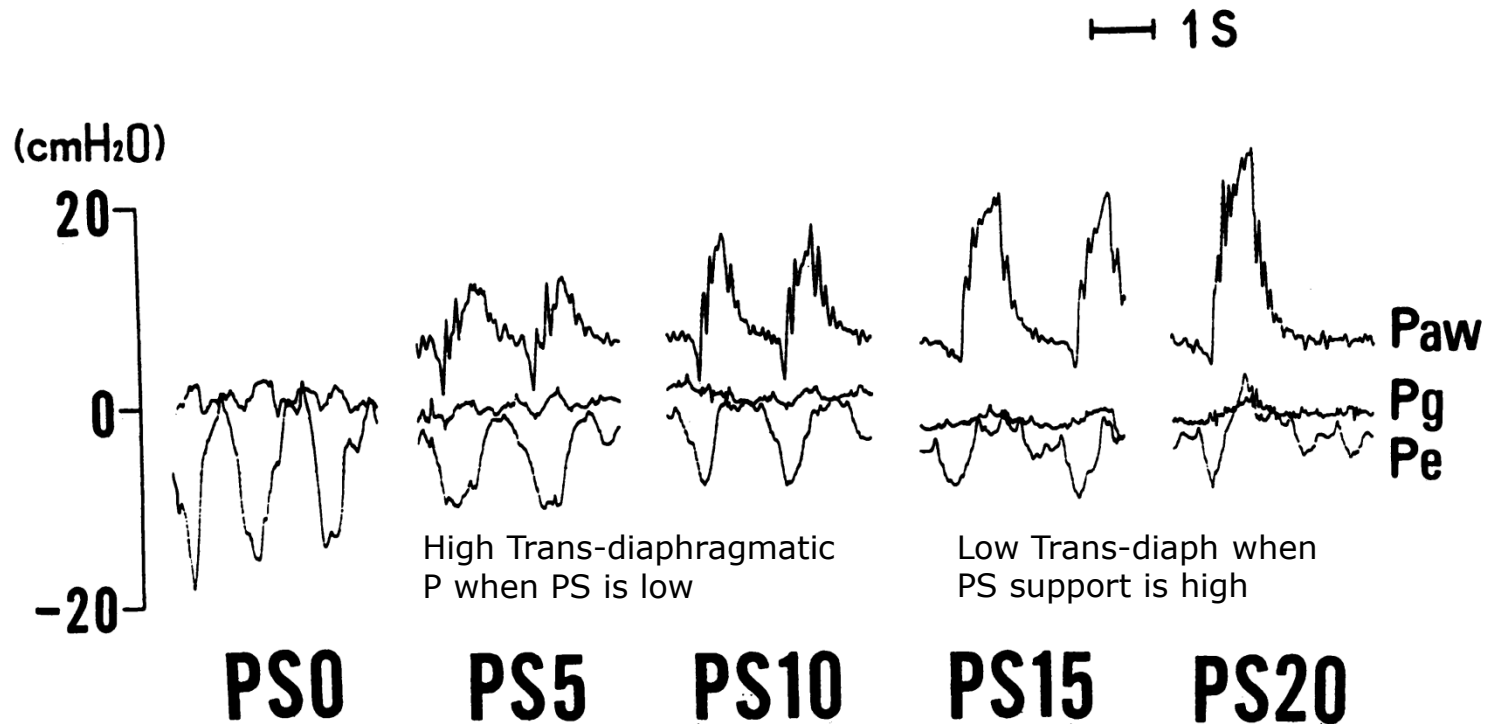
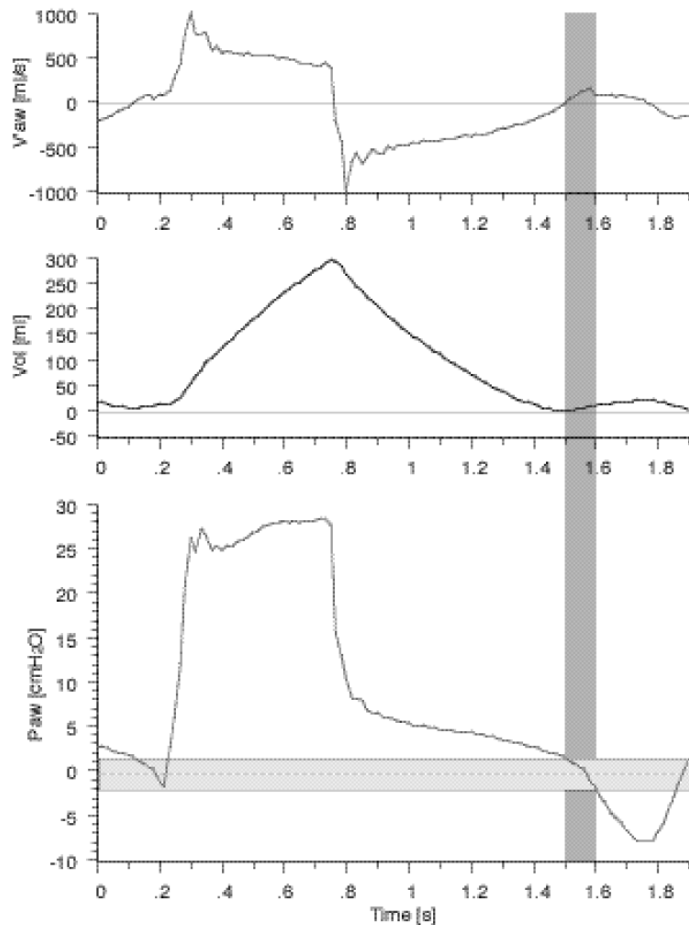


FIGURE 3. Recordings of Paw, Pg, and Pe from five levels of PSV in six patients. Paw in PS0 was deleted because airway was opened. Pe in PS20 was shifted upward at the end of inspiration.

Transdiaphragmatic pressure = $P_{es} - P_{gastric}$
 $P_{gastric}$ is measured by a gastric balloon

Occlusion pressure at 0.1 sec

Measurement of P_{0.1} with a Formal End-Expiratory Occlusion

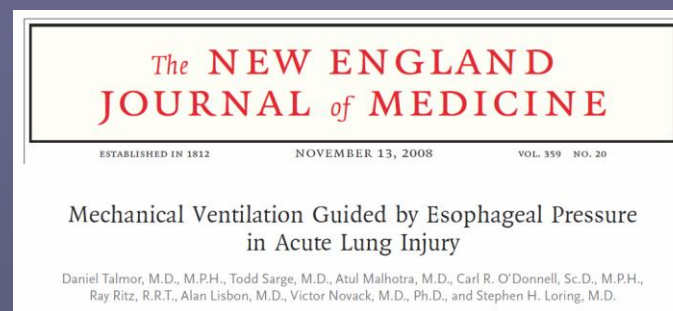
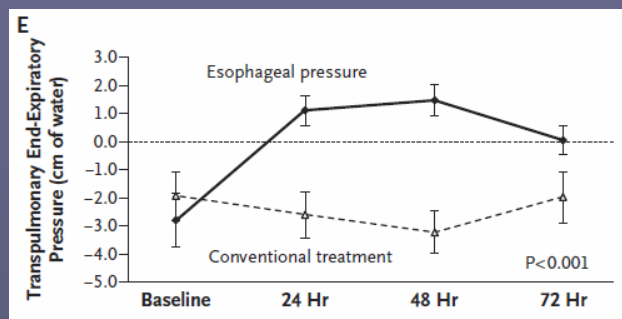


- Corresponds to the drop in P_{aw} , or in P_{es} , observed during the first 100ms of an inspiratory effort performed against the occluded airway opening, with the occlusion performed at the end of exhalation
- In conscious patients, no relevant reaction to an unexpected occlusion before 200ms from start of inspiratory effort
- P_{0.1}: A mechanical index of respiratory drive, directly expresses the force applied by the inspiratory muscles, an index of the motor output of the respiratory centres
- Since gas flow is zero during occlusion, P_{0.1} is independent from resistance and compliance
- Interpretation
 - High: high patient workload and high central respiratory drive
 - Low: if alveolar V normal, then it's normal; if alveolar v is low, it means motor output is low

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Other applications OF respiratory mechanics

Transpulmonary pressure



CONCLUSIONS

As compared with the current standard of care, a ventilator strategy using esophageal pressures to estimate the transpulmonary pressure significantly improves oxygenation and compliance. Multicenter clinical trials are needed to determine whether this approach should be widely adopted. (ClinicalTrials.gov number, NCT00127491.)

The primary endpoint of this study was improvement in oxygenation c/w ARDS Network protocol, not recruitment of decruitment per se.

Critique: absolute value of P_{es} may not be equal to actual P_{pl} , also different at different levels of the lung, cannot be ascertained

Talmor D et al. 2008 NEJM

Summary

1. Basic knowledge: volume, flow, pressure, their derivation and relationship
2. Lung parenchymal condition:
3. Airway condition: FEV1/FVC, Resistance, Flow pattern
4. Chest wall condition: Chest wall compliance
5. Interaction of all factors: PV curve of whole system, Time constant, Flow-time curve, Flow-volume curve, Static and Dynamic hyperinflation, intrinsic PEEP, EELV
6. Work of breathing: Campbell diagram, Pressure-Time Product (PTP)
7. The force of breathing: SVC, FVC, MIP, MEP, Trans-diaphragmatic pressure, P0.1
8. Other application of respiratory mechanics: Transpulmonary pressure

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End

Thank you